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### Poor Correlation, Reproducibility, and Agreement Between Volumetric Versus Linear Epicardial Adipose Tissue Measurement



A 3D Computed Tomography Versus  
2D Echocardiography Comparison

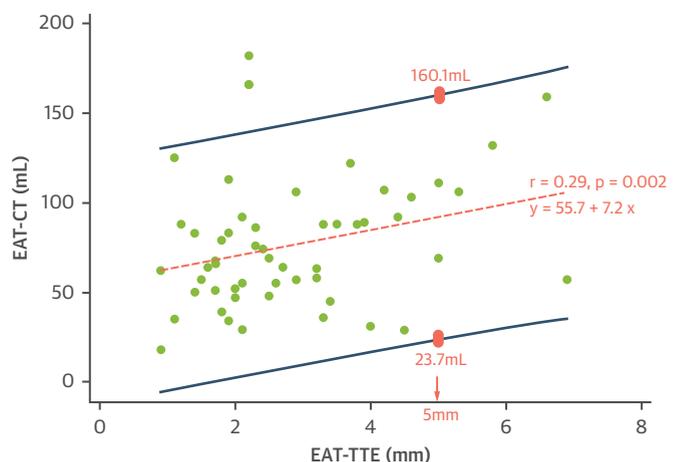
Epicardial adipose tissue (EAT) is a visceral adipose tissue depot and, as such, has been investigated in several metabolic and inflammatory disorders. EAT has been associated with coronary artery disease and myocardial dysfunction, and it remains a burgeoning subject of research due to its potential as a therapeutic target. No endorsed guidelines exist on the measurement of EAT, with studies predominantly reporting linear thickness according to transthoracic echocardiography (EAT-TTE) or area/volume measured by using cardiac computed tomography (EAT-CT). TTE is advantageous because of its rapid performance at the bedside and low cost, but its reproducibility and accuracy may be limited by the effects of probe angulation on 2-dimensional imaging, as well as an inability to quantify periatrial fat or total EAT volume. CT imaging has the drawback of radiation exposure but allows 3-dimensional volumetric quantification. Because EAT is not uniformly distributed around the heart, volumetric quantification is arguably preferred (1). Few data compare agreement between these modalities, and we aimed to compare EAT-TTE versus volumetric EAT-CT by using commonly described methods.

We studied 106 consecutive patients who underwent clinically indicated CT scanning for suspected coronary artery disease who also had TTE performed within 30 days. CT imaging was performed on a 320-row scanner by using a previously described protocol (2), and EAT-CT images were measured by using a research-specific tool (QFAT 2.0, Cedars-Sinai Medical Center, Los Angeles, California) (3). Briefly, EAT was measured from the bifurcation of the pulmonary trunk to the cardiac apex. Manual pericardial contours were drawn at 5- to 10-interval slices with assessment for slice interpolation and corrected as required. Contiguous voxels between -190 and -30 Hounsfield units were used to define and quantify EAT. EAT-TTE was performed by using the technique of Iacobellis et al. (4); EAT was

considered the echo-free space in the parasternal long-axis view between the free wall of the right ventricle and the pericardium. The average value of 3 cycles at end-systole was used with linear measurement along the midline of the ultrasound beam perpendicular to the aortic annulus. Pearson correlation coefficients and linear regression with 95% prediction intervals between methods are reported. Thirty random studies were assessed for interobserver and intraobserver agreement.

EAT-CT compared with EAT-TTE revealed poor correlation ( $r = 0.29$ ;  $p = 0.002$ ), and poor precision was demonstrated by the broad prediction limits (Figure 1). In 28 (26%) cases, observers reported uncertainty as to placement of the linear marker for EAT-TTE, suggesting reduced confidence. When these cases were excluded, correlation was not significantly altered ( $r = 0.25$ ;  $p = 0.01$ ); estimated prediction limits were also not significantly altered (data not shown). Poor interobserver and intraobserver agreement was seen with EAT-TTE (intraclass correlation coefficient [ICC]: 0.39; 95% confidence interval [CI]: 0.04 to 0.65;  $p = 0.02$ ; ICC: 0.56; 95% CI: 0.07 to 0.79;  $p = 0.001$ , respectively); Bland-Altman analysis demonstrated a mean bias of -0.35 mm with 95% limits of agreement from -4.5 to 3.8 mm. Dispersion was particularly evident at

FIGURE 1 Scatter Plot Between EAT-CT and EAT-TTE



The pink dashed line represents the regression line of best fit. R value is the correlation coefficient, and the regression equation is the epicardial adipose tissue area/volume measured by using cardiac computed tomography (EAT-CT) as the outcome variable (y) and epicardial adipose tissue linear thickness according to transthoracic echocardiography (EAT-TTE) as the independent variable (x). The dark blue lines represent 95% prediction intervals. An example is illustrated by the pink boxes: when EAT-TTE is 5 mm, the predicted EAT-CT is between 23.7 and 160.1 mL, representing wide variability and suggesting poor precision.

higher EAT thickness measurements. Conversely, excellent ICC was noted for EAT-CT (ICC: 0.99; 95% CI: 0.98 to 1.00;  $p < 0.001$  for both interobserver and intraobserver) with a mean bias of 0.9 ml and 95% limits of agreement of  $-11.6$  to  $13.4$  ml.

There is significant research interest in EAT-TTE, with its proponents advocating the benefits of easy bedside assessment. However, the poor reproducibility and uncertainty of measurement require caution in drawing associative or causative relationships with EAT. The difference of approximately 8 mm in interrater EAT-TTE, and corresponding wide prediction limits for EAT-CT, may have significant implications in patient misclassification. There are no well-conducted studies comparing imaging-measured EAT versus human autopsy specimens, likely due to the extreme adherence of EAT to the underlying myocardium. However, CT scanning allows adipose tissue thresholding, optimal spatial resolution for pericardium identification, and high reproducibility regardless of the use of iodinated contrast (5).

In conclusion, EAT-CT is highly reproducible compared with EAT-TTE and could be considered as the optimal reference standard for EAT-based research.

**Nitesh Nerlekar, MBBS, MPH\***

**Yi-Wei Baey, MBBS**

**Adam J. Brown, MD, PhD**

**Rahul G. Muthalaly, MBBS, MPH**

**Damini Dey, PhD**

**Balaji Tamarappoo, MD, PhD**

**James D. Cameron, MD, MEngSc**

**Thomas H. Marwick, MBBS, MPH, PhD**

**Dennis T. Wong, MBBS, MD, PhD**

\*Monash Cardiovascular Research Centre and MonashHeart  
Monash Health

246 Clayton Road

Clayton, Victoria 3168

Australia

E-mail: [nitesh.nerlekar@monash.edu](mailto:nitesh.nerlekar@monash.edu)

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## v-net

Deep Learning for Generalized Biventricular Mass and Function Parameters Using Multicenter Cardiac MRI Data



Cardiac magnetic resonance imaging-derived biventricular mass and function parameters, such as end-systolic volume, end-diastolic volume, ejection fraction, stroke volume (SV), and ventricular mass, are clinically well established. Image segmentation can be challenging and time-consuming.

This study introduces v-net (/nju:net/), a deep learning approach facilitating fully automated, high-quality segmentation of the right ventricular (RV) and left ventricular (LV) endocardium and epicardium for reliable and precise estimation of cardiac mass and function parameters.

The study used datasets from Hannover Medical School (MHH), the Data Science Bowl Cardiac Challenge (DSBCC), the MICCAI 2009 LV Segmentation Challenge (LVSC), and the Right Ventricle Segmentation Challenge (RVSC). Training was accomplished on a small subset of the MHH ( $n = 193$ ) and DSBCC ( $n = 60$ ) datasets. Evaluation was performed on all available datasets: MHH ( $n = 309$ ), DSBCC ( $n = 602$ ), LVSC ( $n = 88$ ), and RVSC ( $n = 32$ ). Training and evaluation datasets were mutually exclusive. The network topology was based on U-Net (1). For LV ejection fraction, the single fixed rater intraclass correlation coefficient (ICC) of v-net to ground truth was 0.98 (MHH), 0.95 (LVSC), and 0.80 (DSBCC); for RV ejection fraction, it was 0.96 (MHH) and 0.87 (RVSC); for LV mass, it was 0.95 (MHH) and 0.94 (LVSC); for RV mass, it was 0.83 (MHH and RVSC); for LV SV, it was 0.98 (MHH), 0.91 (LVSC), and 0.90 (DSBCC); and for RV SV, it was 0.92 (MHH) and 0.84 (RVSC). Caudron et al. (2) report a human-level LV ejection fraction ICC of 0.95, an RV ejection fraction of 0.80, an LV mass of 0.85, an RV mass of 0.54, an LV SV of 0.87, and an RV SV of 0.81.

v-net achieves an LV Dice similarity coefficient (DSC) of  $95 \pm 2\%/92 \pm 4\%$  (MHH epicardium/MHH